

**IMPACT OF A DYNAMIC ORTHOSIS ON MANUAL  
DEXTERITY IN PARKINSON'S DISEASE. A RANDOMISED  
TRAIL (Author's final version – Accepted Manuscript)**

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10

11 **Running title:** Dynamic upper limb orthosis in Parkinson

12

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19 **Abstract**

20 **Importance:** Dynamic elastomeric fabric orthosis (DEFO) could be a novel non-  
21 pharmacological treatment for motor symptoms in Parkinson's Disease. **Objective:** To  
22 evaluate the efficacy of the orthoses in manual dexterity in Parkinson's Disease.

23 **Design:** A randomized trial with 20 participants in the control group and 40 in the  
24 experimental group (N=60). Manual dexterity was assessed in ON/OFF states of the  
25 disease with and without the orthosis. **Setting:** Burgos University Hospital.

26 **Participants:** Consecutive non-probabilistic sampling. Inclusion criteria: patients  
27 diagnosed with Parkinson's Disease, with motor symptoms in at least one upper limb,  
28 and attending the neurology department of the Hospital. Age between 48 to 89, with an  
29 average disease duration of  $5.38 \pm 4.23$  years. Exclusion criteria: tremor due to another  
30 neurological disease and/or Montreal Cognitive Assessment score lower than 26.

31 **Intervention:** Implementation of the orthosis on the most affected upper limb for two  
32 months, control group participants did not receive the orthosis. **Outcomes and**

33 **Measures:** Manual dexterity was measured with the Purdue Pegboard Test, Minnesota  
34 Manual Dexterity Test, and Square Test. The paired t-test for related samples and  
35 ANCOVA tests were used. **Results:** Improvements in some items of manual dexterity

36 were observed while wearing the orthosis. However, the improvement was not sustained

37 when the orthosis was removed after two months of use. **Conclusions and Relevance:**

38 This orthosis may improve certain aspects of manual dexterity in people with PD and

39 the patient's functionality, but only while it is worn. **What this article adds:** A dynamic

40 orthosis can reduce the motor symptoms of Parkinson's Disease and improves upper

41 limb functionality.

42 **Keywords:** Parkinson's Disease; non-pharmacological treatment; dynamic elastomeric  
43 fabric orthosis; motor symptoms; manual dexterity.

44 **1. Introduction**

45 Parkinson's Disease (PD) common motor symptoms such as muscle rigidity, tremors,  
46 bradykinesia and impairments in manual dexterity, significantly impact the patient's  
47 ability to perform activities of daily living (ADL) requiring fine motor skills and the  
48 quality of life (QoL) (Bloem et al. 2021a).

49 A decline in manual dexterity, defined as the skill and precision in hands and fingers  
50 fine and coordinated movements, impacts the functional use of the upper limb (UL) in  
51 tasks like reaching, grabbing, and manipulating objects (Heffner & Masterton, 1983;  
52 Poirier, 1988). Manual dexterity serves as a strong predictor of the levels of functional  
53 independence for PD patients (Bloem et al., 2021b; Poewe et al., 2017).

54 The primary approach to motor symptoms in PD is pharmacological, primarily with  
55 levodopa and dopamine agonists. Although medication temporarily improves  
56 symptoms, there is currently no cure for PD (Connolly & Lang, 2014). Over time,  
57 patients often develop motor complications such as dyskinesia and fluctuations in  
58 medication response, limiting the long-term effectiveness (Choi et al., 2017).

59 In most cases, PD treatment is multifaceted, combining pharmacological treatment with  
60 other non-pharmacological approaches to improve the patient's QoL. Various non-  
61 pharmacological interventions such as exercise, acupuncture, and physiotherapy, among  
62 others have been developed, with exercise especially showing improvements in QoL  
63 (Ahn et al., 2017; Van de Weijer, Hommel et al., 2018).

64 Innovative non-pharmacological therapies, such as Motor Imagery, Action Observation,  
65 Dual Therapy, Virtual Reality, and Robot-Assisted Therapy, are emerging in PD to  
66 address functional issues, though there remains a lack of studies and uncertainty  
67 regarding the optimal intervention dosage for effectiveness (Fusco et al., 2019; Righi et

68 al., 2022; Ryan et al., 2021; Strouwen et al., 2015; B. Wang et al., 2019). While some  
69 orthoses have proven effective in reducing motor symptoms in the UL, existing devices  
70 are often bulky and heavy, resulting in low treatment adherence (Fromme, Camenzind,  
71 Riener, & Rossi, 2019).

72 Dynamic Elastomeric Fabric Orthoses (DEFO) are custom-made Lycra garments  
73 individually designed that provide traction forces, aligning the limb biomechanically,  
74 leading to reduced muscle tone and edema; and improved proprioception (Betts, 2015;  
75 González-Bernal et al., 2017). They can be crafted as individual gloves or sleeves, full-  
76 body suits, vests, or ankle-foot wraps (Betts, 2015; Powell et al., 2021). While DEFO  
77 has proven effective in conditions like stroke, pediatric cerebral palsy, multiple  
78 sclerosis, and complex regional pain syndrome, with positive results in motor function,  
79 muscle strength, manual dexterity, and reach (Alexander et al., 2022; Giray et al., 2020;  
80 Miller et al., 2016), its effectiveness in PD remains uncertain.

81 The main goal of Occupational Therapy (OT) is to promote and enable meaningful  
82 contextual occupational performance. The impairment in fine motor skills in PD leads  
83 to a decline in the patient's ADL performance and independence. Therefore, due to the  
84 lack of devices or treatments and the promising research on DEFO in other neurological  
85 conditions, the aim of this study is to assess the effectiveness of this device on manual  
86 dexterity in the UL of PD patients.

87

## 88 2. Method

### 89 2.1. Participants

90 A longitudinal study was undertaken involving a control group (CG) and an  
91 experimental group (EG). Recruitment of patients diagnosed with PD at any stage and

92 experiencing motor symptoms in at least one UL took place between September and  
93 October 2021 through consecutive non-probabilistic sampling at the neurology  
94 department of the University Hospital of Burgos. Exclusion criteria comprised tremor  
95 resulting from another neurological disease and/or a Montreal Cognitive Assessment  
96 (MoCA) score equal to or lower than 26 (Postuma et al., 2015a).

97 PD diagnosis was based on criteria established by the International Parkinson and  
98 Movement Disorder Society, requiring the presence of bradykinesia along with rigidity,  
99 resting tremor, or both. Additionally, at least two out of four supportive criteria  
100 (dramatic improvement from dopaminergic therapy, dyskinesias or loss of smell, resting  
101 tremor, or cardiac sympathetic denervation on myocardial scintigraphy) needed to be  
102 met (Armstrong & Okun, 2020; Postuma et al., 2015b).

103 The study adhered to ethical principles outlined in the Helsinki Declaration, and  
104 participants provided informed consent. It was approved by the Clinical Research Ethics  
105 Committee of the Health Area of Burgos and Soria (Spain) with reference CEIM-  
106 2119/2019; and registered on ClinicalTrials.gov under the test number NCT04815382.

## 107 2.2. Procedure

108 The sample size calculation was based on the improvement in rigidity and tremor as the  
109 main variables. With an alpha risk of 0.05 and a beta risk of 0.20, using a two-tailed test,  
110 it was estimated that 40 participants (20 each group) would be needed to detect a  
111 minimum difference of 0.50 in rigidity and tremor of the most affected UL using Part III  
112 of the Motor Subscale of the Unified Parkinson's Disease Rating Scale (UPDRS)  
113 (Winter et al., 2022). Finally, due to the availability and interest of participants, the  
114 number of participants in the EG was increased to 40, leaving a total sample size of  
115 N=60 (EG=40, CG=20).

116 In the first visit, participants who met the established criteria signed the informed  
117 consent. The sociodemographic and clinical data were collected by occupational  
118 therapists. One month prior to DEFO implementation, exact measurements of UL were  
119 taken by an occupational therapist (that was also a physical therapist) to be fitted for the  
120 personalized customization of the orthosis. The professionals who carry it out must be  
121 specifically trained to do so.

122 The orthosis used in this study is an UL limb DEFO that covers the entire arm and  
123 therefore acts on the entire UL providing proprioceptive stimulation. Since tremor in  
124 people with PD subsides with activity, muscle contraction and support; the orthosis aims  
125 to activate the finger extensors, wrist extensors, radial deviators, supinators and external  
126 rotators, thus, the UL limb is positioned with the musculature in contraction as when the  
127 UL is placed in a support and load position. For its manufacturing, CAD/CAM  
128 technology is used combined with traditional manufacturing techniques to guarantee  
129 that each product matches the exact measurements of the patient. The power net  
130 reinforcement panels are strategically placed to position the upper limb in better  
131 postural alignment(Supplementary material 3).

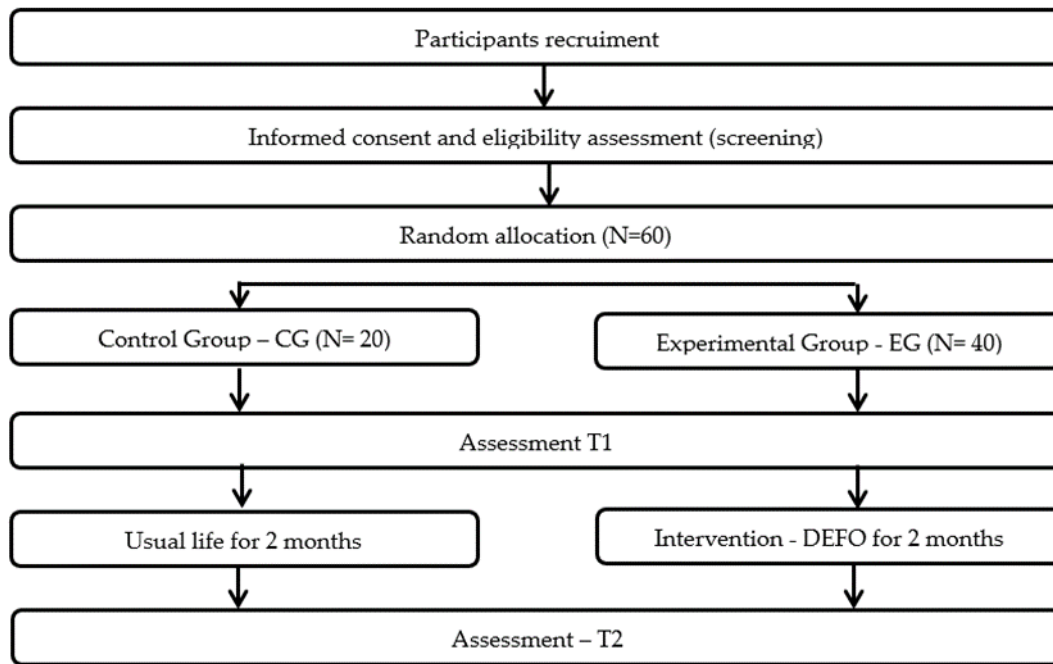
132 Participants were randomly assigned to control group (CG) or experimental group (EG)  
133 with Epidat 4.2 program. The treatment protocol involved implementing the DEFO on  
134 the most affected UL along two months, while participants in the CG continued with  
135 their usual daily activities. The EG participants had to wear the orthosis from the  
136 moment they got up until they went back to bed. They only had to take it off to sleep  
137 and shower. They were instructed to use it in all the activities they usually did and to try  
138 to carry out those activities that they had stopped doing due to their motor symptoms,  
139 such as fishing, sewing or planting. All patients continued with their usual  
140 pharmacological treatment. The effects were evaluated both during the ON state (under

141 the effects of levodopa) and OFF state (1 hour before the next levodopa dose) as there  
142 are significant fluctuations in PD's motor symptoms (Martin, Suchowersky, Kovacs  
143 Burns, & Jonsson, 2010). The ON state refers to periods when medication is effective,  
144 and patients experience significant improvement in their motor function. On the  
145 contrary, the "off" state refers to periods when medication is not effective, and  
146 Parkinson's motor symptoms reappear or worsen significantly, with patients  
147 experiencing increased rigidity, bradykinesia, and tremors. In this research, it is  
148 considered important to evaluate the effect of the DEFO in both states due to the  
149 significant difference in motor symptomatology between them.

150 During the two months of treatment, scheduled calls were made to participants, one  
151 after one week and one after one month of wearing the orthosis, to obtain information  
152 about adherence to treatment; in the two-month evaluation, they were also asked about  
153 this. All participants reported that they have worn the orthosis for the amount of time  
154 indicated.

155 Motor assessments were conducted by occupational therapists at two time points (T1,  
156 T2), immediately prior and following the 2-month intervention window. At both times,  
157 two assessments were performed, one before and one after placing the DEFO, to check  
158 for its immediate effects and its potential long-term benefits (Figure 1). The results were  
159 analyzed by occupational therapists. Neither participants nor evaluators were blinded.

160 **Figure 1.** Study flow chart. DEFO: dynamic elastomeric fabric orthoses.



161

162 Manual dexterity assessment was made following standard testing procedures with three  
 163 different tests: The Purdue Pegboard Test (PPT), the abbreviated version of the  
 164 Minnesota Manual Dexterity Test (MMDT), and the Square Test (ST).

165 Firstly, the PPT consists of a wooden board with 50 holes in two parallel columns, a set  
 166 of pegs, washers, and collars placed in four cups at the top of the board. It has four  
 167 subtests that evaluate the use of the right hand, left hand, alternating movements and the  
 168 combination of both. The score for each subtest is the result of the sum of the pieces  
 169 placed. All subtests were performed three times, and the total score was the average of  
 170 them. Higher scores indicate greater manual dexterity. It is a test with high test-retest  
 171 reliability, with an intraclass correlation coefficient (ICC) of  $\geq 0.90$  (Lo et al., 2022;  
 172 Proud et al., 2019).

173 The MMDT consists of a rectangular board with 60 holes in 15 columns and 4 rows,  
 174 with 60 circular pieces with one side red and other black. It has got two subtests:  
 175 displacement and rotation (supplementary material 1 and 2), that are performed four  
 176 times, with the total score being the average of them. The less time taken in the tests, the



177 better the manual dexterity. It is a reliable and valid measure, with high test-retest  
178 reliability, an intraclass correlation coefficient (ICC) of 0.88, and a 95% confidence  
179 interval (Rane et al., 2017; Y. C. Wang et al., 2018).

180 The ST, which consists of a sheet of paper with four printed grids that consist of 20  
181 squares. The patient is given 30 seconds to make a mark with a pen inside as many  
182 squares as possible. The score is the result of the sum of the marks made without  
183 touching the lines. A higher number indicates better manual dexterity. This is a  
184 reliable and valid test with excellent test-retest reliability for both hands (ICC  $\geq$   
185 0.93) (Soke et al., 2019).

### 186 2.3. Statistical Analysis

187 The data was analyzed using SPSS V28 program considering a p-value  $< 0.05$  as  
188 statistically significant. Mean and standard deviation (SD) were calculated for  
189 quantitative variables, while frequency distribution and percentages for categorical  
190 variables. To analyze the differences between not wearing and wearing the orthosis both  
191 in T1 and T2 in the EG, the paired t-test for related samples was employed; adding in  
192 this case a Bonferroni correction, in order to control for the family-wise error rate  
193 (FWER); for which 4 tests were taken into account as adjustment (2 time points and 2  
194 medication conditions) the corrected p-value obtained was 0.0125 (0.05/4). To analyze  
195 the differences between CG and EG after two months wearing the DAFO, means  
196 between the two groups were compared using ANCOVA, with the group (CG or EG) as  
197 a fixed factor; differential scores of the analyzed variables as dependent variables, and  
198 the pretest scores of each one as covariate. This ANCOVA was performed without  
199 wearing the orthosis. Both t-student test and ANCOVA were performed in ON and OFF  
200 states.

201

202 **3. Results**

203 3.1. Baseline Sociodemographic Characteristics of Participants

204 Sample was composed of 60 individuals with a mean age was 71 years old. 87.5% of  
205 the participants lived with someone (N=53), 10% lived alone in their homes (N=6), and  
206 one person in a religious community. Other sociodemographic data are shown in table 1.

207 **Table 1.** Baseline characteristics

<b>Variables</b>	<b>Total (n= 60)</b>	<b>CG (n= 20)</b>	<b>EP (n = 40)</b>
<b>Age (years)</b>	70.67 ± 10.37	69.94 ± 12.90	70.97 ± 9.32
<b>Gender</b>			
Male	45	14	31
Female	15	5	10
<b>Most affected UL</b>			
Right	35	21	14
Left	25	5	20
<b>Years of disease evolution</b>	4.78 ± 3.83	3.75 ± 2.79	5.21 ± 4.14
<b>Current non-pharmacological treatment</b>			
Physiotherapy	2	0	2
Occupational therapy	0	0	0
Speech therapy	1	1	0
All	1	1	0
None	55	25	30
Others	1	1	0

Abbreviations: CG: Control Group; EP: Experimental Group; UL: Upper limb

208

209 Table 2 shows the observed differences in the comparative analysis of motor dexterity  
210 assessments (PPT, MMDT, and ST) at baseline (T1) with and without the orthosis in  
211 both ON and OFF states.

212 **Table 2.** Comparative analysis of motor dexterity assessment at baseline (T1) with  
213 and without the orthosis. Paired t-test for related samples (N=40)

<b>Variables</b>	<b>State</b>	<b>Mean</b>	<b>SD</b>	<b><math>\alpha</math></b>	<b><math>\alpha_{corrected}</math></b>	<b>p-value</b>
PPT Subtest 1	OFF	.393	1.416	0.05	0.0125	.102
	ON	.606	1.368	0.05	0.0125	<b>.012</b>
PPT Subtest 2	OFF	-.007	1.404	0.05	0.0125	.975
	ON	.073	1.872	0.05	0.0125	.814
PPT Subtest 3	OFF	.024	.949	0.05	0.0125	.879
	ON	.565	1.412	0.05	0.0125	.022
PPT subtest 4	OFF	.042	2.477	0.05	0.0125	.918
	ON	.236	6.423	0.05	0.0125	.827
MMDT placing test	OFF	-6.901	11.305	0.05	0.0125	<b>.001</b>
	ON	-5.424	10.734	0.05	0.0125	<b>.005</b>
MMDT turning test	OFF	1.583	42.367	0.05	0.0125	.826
	ON	2.201	9.943	0.05	0.0125	.193
ST Right hand	OFF	-.971	7.278	0.05	0.0125	.435
	ON	-.417	6.29	0.05	0.0125	.693
ST Left hand	OFF	-.828	7.422	0.05	0.0125	.513
	ON	1.083	4.625	0.05	0.0125	.187

214 Mean: mean difference between the group with and without orthosis. ON: under levodopa  
215 effects; OFF: 1 hour before next levodopa dose; SD: Standard Deviation; PPT: The Purdue  
216 Pegboard Test; MMDT: Minnesota Manual Dexterity Test; ST: Square Test.

217

218 Table 3 presents the observed differences in the comparative analysis of motor dexterity  
219 assessments (PPT, MMDT, and ST) in the evaluation conducted 2 months after the  
220 implementation of the DEFO (T2), both with and without the orthosis in both ON and  
221 OFF states.

222 **Table 3.** Comparative analysis of motor dexterity assessments after 2 months of  
223 the implementation of the DEFO (T2), with and without the orthosis. Paired t-test  
224 for related samples (N=40)

Variables	State	Mean	SD	$\alpha$	$\alpha_{corrected}$	p-value
PPT Subtest 1	OFF	.341	1.31	0.05	0.0125	.064
	ON	.441	1.168	0.05	0.0125	<b>.008</b>
PPT Subtest 2	OFF	-.05	1.053	0.05	0.0125	.733
	ON	.661	3.323	0.05	0.0125	.154
PPT Subtest 3	OFF	.066	1.455	0.05	0.0125	.740
	ON	.534	1.637	0.05	0.0125	.021
PPT subtest 4	OFF	-1.911	24.935	0.05	0.0125	.579
	ON	.887	7.749	0.05	0.0125	.409
MMDT placing test	OFF	-5.185	16.692	0.05	0.0125	.028
	ON	-3.638	13.248	0.05	0.0125	.051
MMDT turning test	OFF	-3.656	19.377	0.05	0.0125	.180
	ON	3.453	11.116	0.05	0.0125	.028
ST Right hand	OFF	2.019	16.056	0.05	0.0125	.369
	ON	-2.642	8.204	0.05	0.0125	.023
ST Left hand	OFF	-1.192	7.667	0.05	0.0125	.267
	ON	.170	6.100	0.05	0.0125	.064

225 Mean: mean difference between the group with and without orthosis. ON: under levodopa

226 effects; OFF: 1 hour before next levodopa dose; SD: Standard Deviation; PPT: The Purdue

227 Pegboard Test; MMDT: Minnesota Manual Dexterity Test; ST: Square Test

228

229 No differences were observed between the CG and the EG in the PPT, in the MMDT or

230 in the ST without orthosis after the EG had worn the orthosis for two months

231 (Supplementary material 4).

232

#### 233 4. Discussion

234 The main results of this study indicate that improvements in certain aspects of motor

235 dexterity occur when the patient wears the orthosis. However, after using the orthosis

236 regularly for two months, no differences were observed in manual dexterity of the UL  
237 when the orthosis was removed.

238 Among motor symptoms, bradykinesia, rigidity, resting tremor, and impaired motor  
239 dexterity are prominent and can manifest themselves in varying degrees as the disease  
240 progresses, but they are highly bothersome and disabling, impacting performance in  
241 ADL and QoL (Bloem et al., 2021b; Postuma et al., 2015a).

242 In recent years, the effectiveness of these devices has been tested in other conditions.  
243 Jen et al. explored their implementation in stroke patients, observing an improvement in  
244 function and dexterity in the UL and promotion of participation in repetitive activities  
245 (Alexander et al., 2021). Studies conducted in cases of cerebral palsy have demonstrated  
246 their effectiveness in improving manual dexterity (Giray et al., 2020; Pavão et al.,  
247 2018), functionality and alignment of the affected UL (Yasukawa & Uronis, 2014).

248 These results partially align with those obtained in the present study as an immediate  
249 effect of the orthosis was observed in some subtests both in T1 and T2. Therefore,  
250 improvements in certain aspects of motor dexterity are observed when the orthosis is  
251 being used. However, after using the orthosis for 2 months, no differences were  
252 observed between CG and EG when the tests are performed without the orthosis, which  
253 may be explained, in part, because while PD is a degenerative condition, stroke and  
254 cerebral palsy are not.

255 Various orthoses tested have shown positive effects on reducing involuntary movement,  
256 but they were also heavy and unattractive, leading to reluctance in their use (Fromme et  
257 al., 2019; Mo & Prierer, 2021). Therefore, there is a need to design lighter and appealing  
258 to the patient orthosis, while also providing an improvement in manual dexterity.

259 This research must be considered in the context of their strengths and limitations.  
260 DEFOs have proven to be easily implementable and adherent devices, resulting in  
261 improvements in some aspects of manual dexterity, both the ON and OFF states of the  
262 disease. Although no differences were found after removing the orthosis in manual  
263 dexterity, improvements were obtained in occupational performance with the orthosis  
264 on. Furthermore, they represent a non-pharmacological treatment without any  
265 contraindications for the patient.

266 In the results, there is a tendency for greater differences to appear between wearing or  
267 not wearing the orthosis in the ON state; however, they lack statistical significance after  
268 applying the Bonferroni correction. At first glance, there does not seem to be an obvious  
269 reason for the medication state to interact with the use of the orthosis in this way;  
270 however, the role of medication state and its interactions with findings should be  
271 addressed more deeply in future research. Understanding the orthosis response in both  
272 states allows for optimizing its use, adjusting the timing to maximize its benefits during  
273 ON periods and minimize symptoms during OFF periods.

274 The observational nature of the study, and not having blinded evaluators or patients are  
275 limitations for this study. Additionally, due to the limited duration of the study, it was  
276 not possible to ascertain whether longer-term treatment might lead to further  
277 improvements or if it could slow down the progressive deterioration of the disease. On  
278 the other hand, although participants reported that they had worn the orthosis for the amount  
279 of time indicated since they were able to perform their activities better, and they did not have as  
280 much tremor; these devices do not include a sensor that allows obtaining objective data  
281 on their adherence, and despite having obtained this information in the telephone calls  
282 made during the intervention period as well as in the evaluation after two months, it  
283 would be interesting to obtain objective data about both adherence and participation.

284 The use of the Bonferroni correction itself has some advantages and disadvantages to  
285 consider. It is easy to apply and understand, and minimizes the risk of false positive  
286 errors, as well as being a robust and conservative adjustment that does not depend on  
287 the nature or distribution of the data or tests and works for any number of tests. On the  
288 other hand, it may be too conservative, reducing the power of each test and increasing  
289 the risk of false negative errors; it is also not flexible, as it does not take into account the  
290 dependence or correlation between tests. All of this must be taken into account when  
291 interpreting the results obtained in this research, since when applying the corrected  $\alpha$   
292 value, some results that would be positive at a significance level of 0.05 are lost; this is  
293 something that will have to be addressed in future research.

294 Furthermore, this orthosis was implemented during the winter months in a city with a  
295 cold climate, so it did not give heat to the participants, however it would be interesting  
296 to manufacture it with a breathable material so that heat would not be a problem and  
297 could maintain its adhesion in other warmer climates.

298 Currently, there is a lack of effective orthopedic devices that can be implemented as a  
299 non-pharmacological treatment in PD. The results obtained in the present study can be a  
300 starting point to continue researching these devices in PD or encourage the development  
301 of new ones that are easy to implement, lightweight, and with patient adherence, in  
302 order to improve manual dexterity and thus allow greater participation in ADLs,  
303 improving their functionality and quality of life. Given that no effects were found when  
304 the device was removed, in a future, for a longer implementation of the orthosis for  
305 months, it could be interesting to wear it only while performing those activities that are  
306 relevant to the patient. Furthermore, given that the biggest problem with current  
307 orthoses is their lack of adherence because they are heavy, it would be interesting to

308 implement a sensor that allows checking the adherence in this orthosis and having  
309 objective data about it.

310 Although no differences were found in manual dexterity after removal of the orthosis, it  
311 is possible that differences could occur in other variables not studied such as  
312 occupational performance, daily use of the arm and hand, etc., which would be  
313 interesting variables for future research.

314

## 315 **5. Implications for Occupational Therapy Practice**

316 Currently, PD's fundamental treatment is pharmacological; however, OT is of great  
317 relevance for the patient's occupational performance and QoL. Studies such as this one  
318 can encourage greater involvement of occupational therapy in this and other populations. This  
319 research shows an alternative non-pharmacological treatment that could reduce the  
320 motor symptoms, improve patients' functionality, and increase their QoL without  
321 adverse side effects.

322 In clinical practice, the implications of implementing DEFO could lead to a reduction in  
323 bothersome motor symptoms like tremors and rigidity, thereby enhancing functionality  
324 fostering greater autonomy for patients in their daily lives. Moreover, such interventions  
325 have the potential to substantially improve the quality of life (QoL) for patients,  
326 fostering a positive self-image and reducing embarrassment and insecurity associated  
327 with symptoms like tremors. By enabling individuals to participate more fully in social  
328 activities and group outings without fear of functional limitations, these interventions  
329 could enhance social integration and rekindle interest in activities that patients may have  
330 previously abandoned. This, in turn, could bolster motivation to explore new activities



331 and experiences without the burden of apprehension or the fear of failure, ultimately  
332 promoting a more fulfilling and enriching lifestyle for patients.

333

## 334 **5. Conclusions**

335 The DEFO is an easy-to-implement device that may improve manipulative dexterity  
336 when worn, and therefore may be a non-pharmacological adjunct to standard treatment  
337 to improve the motor aspects of the disease.

338 As few studies have been conducted with the DEFO in PD, further research is needed to  
339 verify its efficacy in PD as well as to see if these possible improvements in  
340 manipulative dexterity translate into improvements in occupational performance and  
341 participation. Also, including treatment adherence variables in future research would  
342 also be of interest.

343

## 344 **Author Contributions**

345 Conceptualization, J.G.-S., E.C., M.J.-B. and J.M.T.G.-G.; methodology, J.G.-B. and  
346 M.J.-B. ; software, J.G.-B. and J.M.T.G.-G.; validation, E.C. and J.M.T.G.-G.; formal  
347 analysis, M.J.-B., M.S.-P. and J.G.-B.; investigation, M.J.-B., C.C.-R. and M.S.-P.;  
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359 **Institutional Review Board Statement**

360 The study was conducted in accordance with the Declaration of Helsinki and approved  
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364 **Informed Consent Statement**

365 Informed consent was obtained from all subjects involved in the study.

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496 **Supplementary material 1.**

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499 **Supplementary figure 1.** Patient performing the displacement subtest with the  
500 DEFO. Own-made source

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513 **Supplementary material 2.**



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515 **Supplementary figure 2.** Patient performing the rotation subtest with the DEFO.  
516 Own-made source

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### 530 **Supplementary material 3. DEFO FABRICATION OVERVIEW**

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532 Dynamic elastomeric fabric orthoses (DEFO) are used to address the physical  
533 symptoms associated with neurological, genetic, and musculoskeletal disorders. These  
534 orthoses employ a soft, flexible, and durable compression fabric aimed at realigning the  
535 affected body segment and influencing muscle tone and the proprioceptive system.  
536 Custom-made for a precise fit, each orthosis applies pressure to the affected areas via  
537 strategically positioned powernet reinforcement panels.

538 DEFO are garments that integrate an elastic material with biomechanical reinforcement  
539 panels, serving two main functions:

- 540 1- They enhance proprioception by stimulating the body's sensory systems.
- 541 2- The reinforcement panels realign the body and provide stability at a  
542 biomechanical level.

543 For movement control, appropriate stimuli are required (tremor in Parkinson's disease is  
544 an example of involuntary movements in the extrapyramidal pathway). DEFO stimulate  
545 the somatosensory system through the proprioceptors in the musculoskeletal system.  
546 This sensory information is processed by the cerebellum to adjust movements and  
547 posture, influence muscle tone, and provide proximal stability. Different regions of the  
548 cerebral cortex then interpret these sensations in meaningful ways, leading to improved  
549 movement. Consequently, DEFO can be utilized in both neurophysiological and  
550 biomechanical therapies.

551 Measurements are taken using specific forms that therapists learn to use during  
552 specialized training, ensuring the orthoses fit correctly without being too tight or too  
553 loose. These measurements are performed while the patient is seated, using a series of  
554 precise reference points on the upper limb.

555 The DEFO are created after taking precise measurements to design the base garment, in  
556 this case, an orthosis for the upper limb, always aiming for a functional position. From  
557 this position, measurements are taken for the necessary reinforcements, based on the  
558 desired outcome. In the context of reducing tremor in individuals with Parkinson's  
559 disease, the objective was to activate the finger extensors, wrist extensors, radial  
560 deviators, supinators, and external rotators. This approach positions the upper limb with  
561 muscles contracting as they would when the limb is supported and bearing weight.

562 The reinforcements designed to achieve this effect include:

- 563 - External rotation reinforcement: panel to sleeve used to correct internal rotation  
564 of the shoulder/arm.
- 565 - Radial side reinforcement: from the base of the thumb to correct ulnar deviation
- 566 - Arm tremor proximal reinforcement: designed to reduce forearm tremor by  
567 applying pressure to the deep muscles of the upper forearm

568 - Thumb abduction reinforcement: from the proximal thumb joint on the palmar  
569 aspect, across the posterior of the wrist, to the ulnar aspect of wrist joint; to correct  
570 excessive thumb adduction.

571 - Elbow flexion angle reinforcement: specifies the required degree of elbow  
572 flexion with the arm in the patient's natural resting position.

573 Additional reinforcements can be applied to increase traction as needed. The prescribing  
574 professional determines which reinforcements are necessary for each case based on their  
575 training.

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578 **Imagen:** Dynamic elastomeric fabric orthose (DEFO).

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593 **Supplementary material 4.** Inter-group comparison of PPT, MMDT and ST differential score evaluation T2 without orthoses in ON  
 594 and OFF state. ANCOVA

	<b>Variables</b>	<b>Group</b>	<b>Mean</b>	<b>SD</b>	<b>MS</b>	<b>F</b>	<b><i>p-value</i></b>	<b><math>\eta^2</math></b>
PPT Subtest 1	ON – without orthoses	CG	.076	1.29	.489	.232	.632	.005
		EG	-.175	1.50				
	OFF – without orthoses	CG	.111	1.219	.976	.019		
		EG	.189	1.803				
PPT Subtest 2	ON – without orthoses	CG	.446	1.258	2.458	.139	.711	.003
		EG	.934	5.317				
	OFF – without orthoses	CG	.40	1.57	.898	.416		
		EG	.116	1.425				
PPT Subtest 3	ON – without orthoses	CG	.177	1.323	4.587	.507	.480	.010
		EG	.873	3.479				
	OFF – without orthoses	CG	.001	1.194	12.132	1.137		
		EG	1.069	3.790				
PPT Subtest 4	ON-without orthoses	CG	-.1000	5.280	38.460	.410	.525	.008
		EG	1.793	11.674				
	OFF-without orthoses	CG	-.222	1.250	40.381	3.664		
		EG	1.707	3.785				
MMDT Placing test	ON – without orthoses	CG	.347	27.380	2.171	.005	.943	.000
		EG	1.392	17.442				
	OFF – without orthoses	CG	3.256	24.600	365.771	.745		
		EG	-2.574	20.840				
MMDT Turning test	ON – without orthoses	CG	-6.967	17.023	424.270	1.721	.196	.033
		EG	-.454	14.993				
	OFF – without orthoses	CG	.033	9.911	210.418	.313		

		EG	-6.270	37.093				
ST Right hand	ON – without orthoses	CG	2.933	9.706	157.431	1.725	.195	.033
		EG	-1.132	9.416				
	OFF – without orthoses	CG	-.333	9.693	588.302	2.089	.155	.041
		EG	7.108	18.625				
ST Left hand	ON-without orthoses	CG	2.133	6.346	28.048	.365	.548	.007
		EG	-.026	9.774				
	OFF-without orthoses	CG	6.949	6.949	310.548	3.417	.071	.065
		EG	10.534	10..535				

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PPT: Purdue Pegboard Test; MMDT: Minnesota Manual Dexterity Test; ST: Square Test; CG: Control group (n=20), EG: experimental group (n=40), SD: standard deviation, p value < .05